

# Noise

In electromagnetic systems, the energy per photon =  $h\nu$ .

In communication systems, noise can be either **quantum** or **additive** from the measurement system ( receiver, etc).

The **additive** noise power is  $4kTB$ ,

$k$  is the Boltzman constant

$T$  is the absolute temperature

$B$  is the bandwidth of the system.

When making a measurement (e.g. measuring voltage in a receiver), noise energy per unit time  $1/B$  can be written as  $4kT$ .

$$SNR = \frac{Nh\nu}{\sqrt{Nh\nu + AdditiveNoise}} = \frac{Nh\nu}{\sqrt{Nh\nu + 4kT}}$$

$\sqrt{N}$  comes from the standard deviation of the number of photons per time element.

# SNR in x-ray systems

$$SNR = \frac{Nh\nu}{\sqrt{Nh\nu + AdditiveNoise}} = \frac{Nh\nu}{\sqrt{Nh\nu + 4kT}}$$

When the frequency  $\nu \ll \text{GHz}$ ,  $4kT \gg h\nu$

In the X-ray region where frequencies are on the order of  $10^{19}$ :

$$h\nu \gg 4kT$$

X-ray is quantum limited due to the discrete number of photons per pixel.

We need to know the mean and variance of the random process that generate x-ray photons, absorb them, and record them.

$$\text{Recall: } h = 6.63 \times 10^{-34} \text{ Js}$$

$$k = 1.38 \times 10^{-23} \text{ J/K}$$

# Discrete-Quantum Nature of EM radiation detection

- Detector does not continuously absorb energy
- But, absorb energy in increments of  $h\nu$
- Therefore, the output of detector cannot be smooth
- But also exhibit Fluctuations known as quantum noise, or Poisson noise (as definition of Poisson distribution, as we see later)

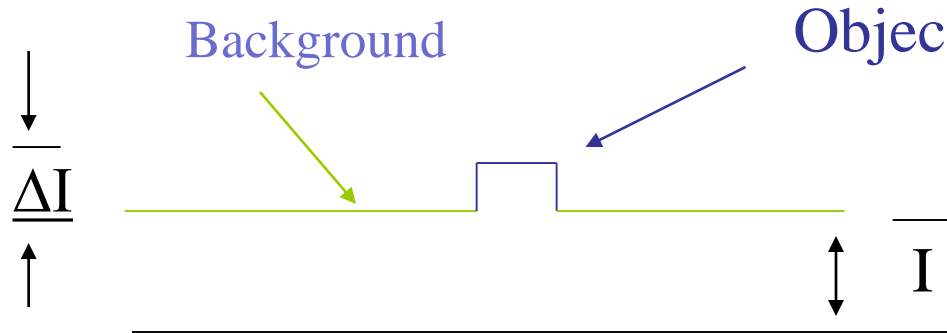
# Noise in x-ray system

- $h\nu$  is so large for x-rays due to necessity of radiation dose to patient, therefore:
  - 1) Small number of quanta is probable to be detected
  - 2) Large number of photons is required for proper density on Film
    - $10^7$  x-ray photons/cm<sup>2</sup> exposed on Screen
    - $10^{11}$ - $10^{12}$  optical photons/cm<sup>2</sup> exposed on Film
- Therefore, with so few number of detected quanta, the quantum noise (poisson fluctuation) is dominant in radiographic images

# Assumptions

- Stationary statistics for a constant source and fixed source-detector geometry
- Ideal detector which responds to every phonon impinging on it

# Motivation:



$$\text{Contrast} = \Delta I / \bar{I}$$

$$\text{SNR} = \Delta I / \sigma_I = \bar{C} \bar{I} / \sigma_I$$

We are concerned to detect some objects (here shown in blue) that have a different property, e.g. “attenuation”, from the background (green).

To do so:

we have to be able to describe the **random processes** that will cause the x-ray intensity to vary across the background.

## binomial distribution:

is the discrete probability distribution of the number of successes (eg. Photon detection) in a sequence of  $n$  independent experiments (# of interacting photons). Each photon detection yields success with probability  $p$ .

If experiment has only 2 possible outcomes for each trial (eg. Yes/No), we call it a Bernouli random variable.

Success: Probability of one is  $p$

Failure: Probability of the other is  $1 - p$

## Rolling dies

**P**

The outcome of rolling the die is a random variable of discrete values.

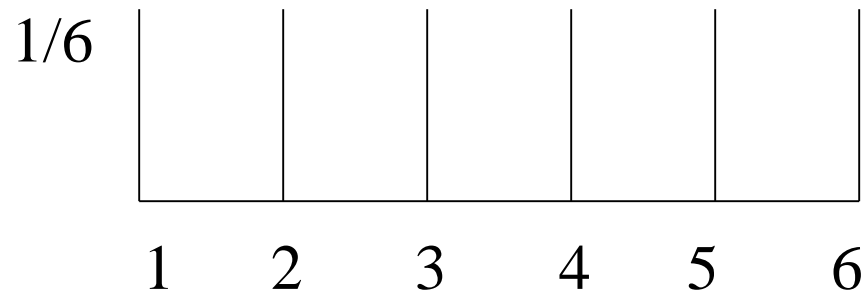
**r**

Let's call this random variable  $X$ . We write then that the probability of  $X$  being value  $n$  (eg. 2) is  $p_x(n) = 1/6$

**o**

**b**

**a**



**b**

**i**

**i**

**i**

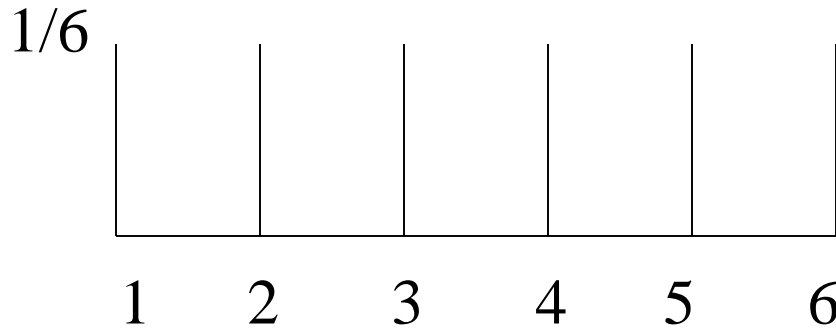
**t**

Note: Because the probability of all events is equal, we refer to this event as having a **uniform** probability distribution

**y**

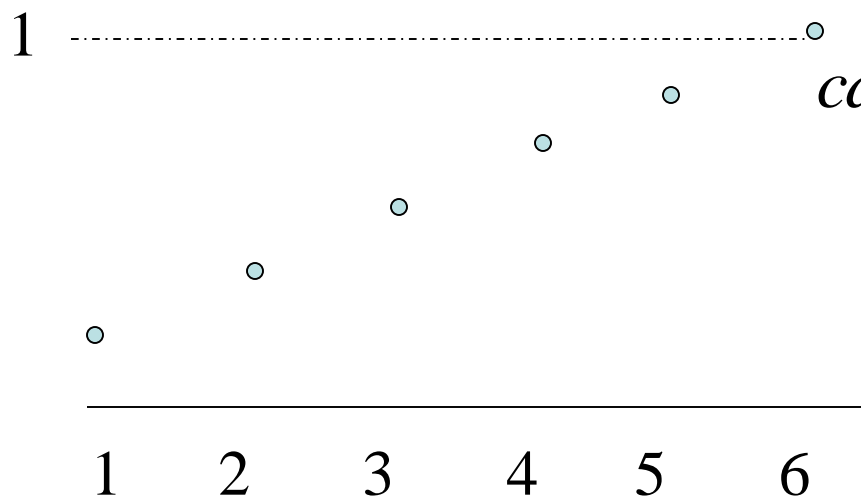


# Probability Density Function (pdf)



$$p_X(j) = \frac{1}{6}$$

# Cumulative Density Function



$$cdf(m) = F_x(x) = \sum_{j=1}^{j=m} p_X(j)$$

pdf is derivative of cdf:

$$p_X(x) = dF_X(x) / dx$$

$$0 \leq F_X(x) \leq 1$$

**P**  
**r**  
**o**  
**b**  
**a**  
**b**  
**i**  
**i**  
**t**  
**y**

# Zeroth Order Statistics

- Not concerned with relationship between events along a random process
- Just looks at one point in time or space
- Mean of  $X$ ,  $\mu_X$ , or Expected Value of  $X$ ,  $E[X]$

– Measures first moment of  $p_X(x)$        $\mu_X = \int_{-\infty}^{\infty} xp_X(x)dx$

- Variance of  $X$ ,  $\sigma^2_X$ , or  $E[(X-\mu)^2]$

– Measure second moment of  $p_X(x)$        $\sigma_X^2 = \int_{-\infty}^{\infty} (x - \mu)^2 p_X(x)dx$

Standard deviation

$$\sigma_X = std$$

# Zeroth Order Statistics

- Recall  $E[X] = \int_{-\infty}^{\infty} xp_X(x)dx$
- Variance of X or  $E[(X-\mu)^2]$

$$\sigma_X^2 = \int_{-\infty}^{\infty} (x - \mu)^2 p_X(x) dx$$

$$\sigma_X^2 = \int_{-\infty}^{\infty} x^2 p_X(x) dx - 2\mu \int_{-\infty}^{\infty} x p_X(x) dx + \mu^2 \int_{-\infty}^{\infty} p_X(x) dx$$

$$\sigma_X^2 = E[X^2] - 2\mu E[X] + \mu^2$$

$$\sigma_X^2 = E[X^2] - E^2[X] = E[X^2] - \mu^2$$

# Binomial Random Variable

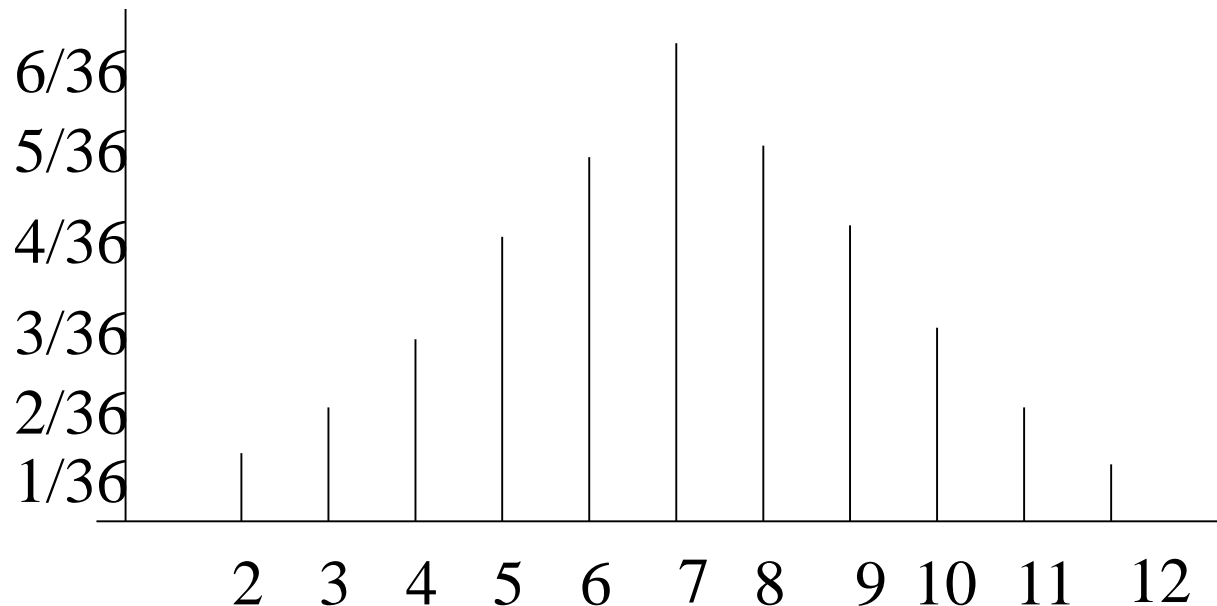
$p(j)$  for throwing 2 die is  $1/36$ :

Let die 1 experiment result be  $x$  and called Random Variable  $X$

Let die 2 experiment result be  $y$  and called Random Variable  $Y$

With independence:  $p_{XY}(x,y) = p_X(x) p_Y(y)$

$$E[xy] = \int \int xy p_{XY}(x,y) dx dy = \int x p_X(x) dx \int y p_Y(y) dy = E[X] E[Y]$$



# Other helpful Theorems

$$E[X+Y] = E[X] + E[Y] \text{ Always}$$

$$E[aX] = aE[X] \text{ Always}$$

$$\sigma_x^2 = E[X^2] - E^2[X] \text{ Always}$$

$$\sigma^2(aX) = a^2 \sigma_x^2 \text{ Always}$$

$$E[X + c] = E[X] + c$$

$$\text{Var}(X + Y) = \text{Var}(X) + \text{Var}(Y) \text{ only if the } X \text{ and } Y \\ \text{are statistically independent.}$$

---

For  $n$  trials,

$P[X = i]$  is the probability of  $i$  successes in the  $n$  trials

$X$  is said to be a binomial variable with parameters  $(n, p)$

$$p[X = i] = \frac{n!}{(n-i)!i!} p^i (1-p)^{n-i}$$

**E**

Roll a die 10 times ( $n=10$ ).

In this game, you win if you roll a 6.

Anything else - you lose

**X**

What is  $P[X = 2]$ , the probability you win twice ( $i=2$ )?

**a**

$$p[X = i] = \frac{n!}{(n-i)!i!} p^i (1-p)^{n-i}$$

**m**

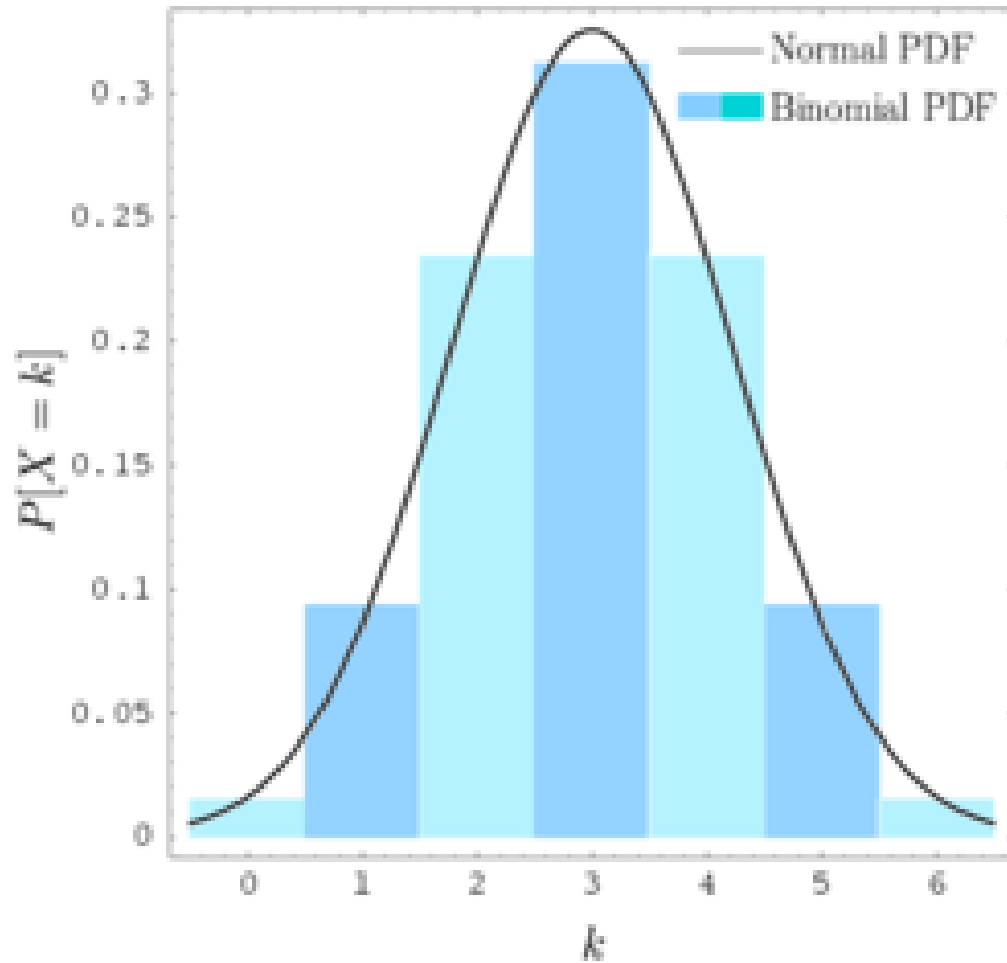
$$= (10! / 8! 2!) (1/6)^2 (5/6)^8$$

**p**

$$= (90 / 2) (1/36) (5/6)^8 = 0.2907$$

**l**

**e**



Binomial PDF and normal approximation  
for  $n = 6$  and  $p = 0.5$ .



## Limits of binomial distributions

- As  $n$  approaches  $\infty$  and  $p$  approaches 0, then the Binomial( $n, p$ ) distribution approaches the Poisson distribution with expected value  $\lambda=np$  .
- As  $n$  approaches  $\infty$  while  $p$  remains fixed, this distribution approaches the normal distribution with expected value 0 and variance 1
- (this is just a specific case of the Central Limit Theorem).

Recall: If  $p$  is small and  $n$  large so that  $np$  is moderate, then an approximate (very good) probability is:

$P[X=i] = e^{-\lambda} \lambda^i / i!$       Where  $np = \lambda$   
the probability exactly  $i$  events happen

## ***Poisson Random Variable***

With Poisson random variables, their mean is equal to their variance!

$$E[X] = \sigma_x^2 = \lambda$$

**E**

Let the probability that a letter on a page is misprinted is  $1/1600$ . Let's assume 800 characters per page. Find the probability of 1 error on the page.

**X**

Using Binomial Random Variable Calculation:

**a**

$i = 1, p = 1/1600$  and  $n = 800$

$$P [ X = 1 ] = (800! / 799!) (1/1600) (1599/1600)^{799}$$

**m**

Very difficult to calculate some of the above terms.

But using Poisson calculation:

**p**

$$P [ X = i ] = e^{-\lambda} \lambda^i / i! \quad \text{Here, so } \lambda = np = 1/2$$

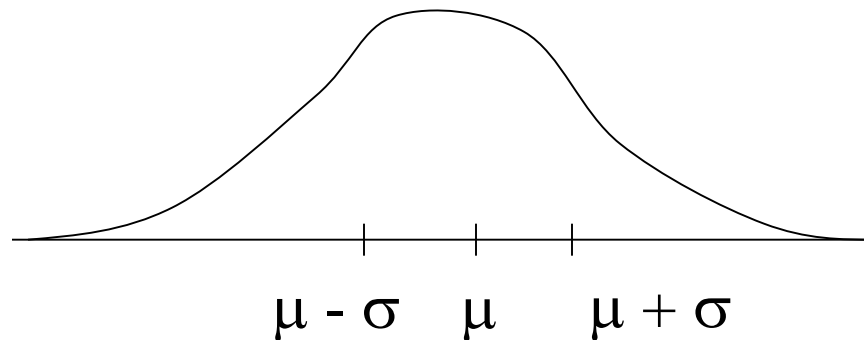
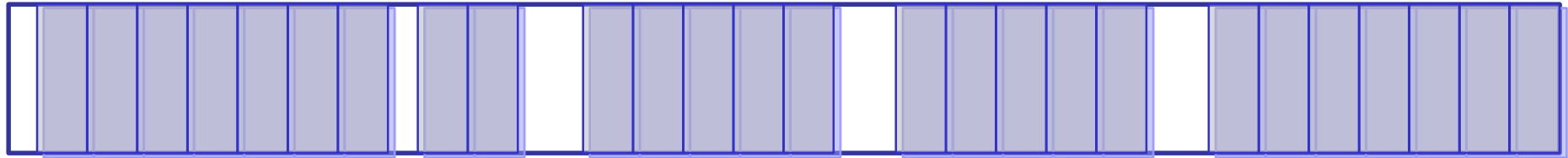
**i**

$$\text{So } P[X=1] = 1/2 e^{-0.5} = .30$$

**E**

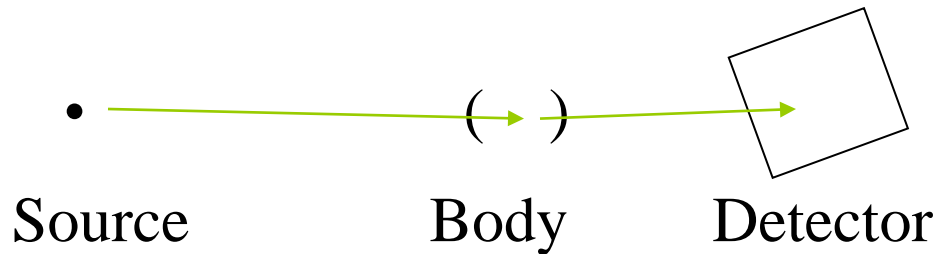
# Other Poisson Random Variables

- 1) Number of biscuits sold in a store each day
- 2) Number of x-rays discharged off an anode



$$p_X(x) = \frac{1}{\sqrt{2\pi}\sigma} \exp\left[-\frac{(x-\mu)^2}{2\sigma^2}\right]$$

To find the probability density function that describes the **number of photons striking on the Detector pixel**



1) Probability of X-ray emission is a Poisson process:

$$P\left(\frac{i_{emissions}}{unit - time}\right) = N_0^i \frac{e^{-N_0}}{i!}$$

$N_0$  is the average number of emitted X-ray photons (i.e  $\lambda$  in the Poisson process).

## 2) Transmission -- Binomial Process

$$\begin{array}{ll} \text{transmitted} & p = e^{-\int u(z) dz} \\ \text{interacting} & q = 1 - p \end{array}$$

## 3) Cascade of a Poisson and Binary Process still has a Poisson Probability Density Function

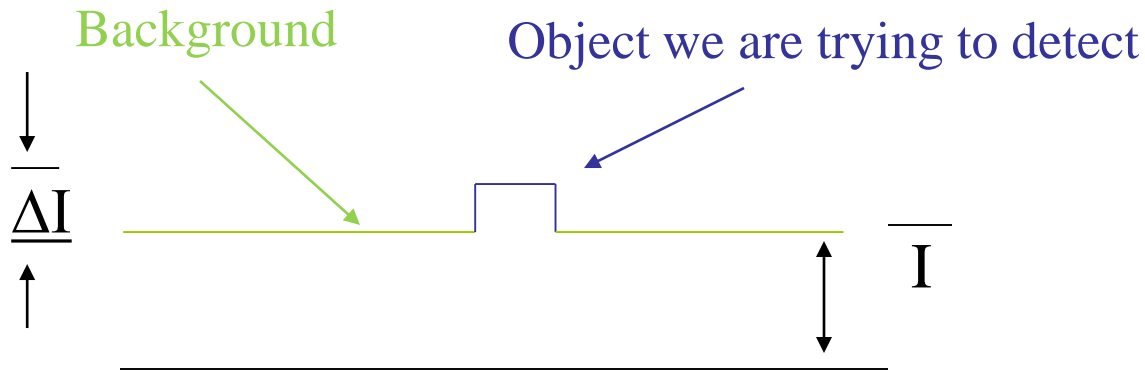
-  $Q(i)$  represents transmission of Emitted photons:

$$Q(i) = (pN_0)^i \frac{e^{-pN_0}}{i!}$$

With Average Transmission:  $\lambda = pN_0$

Variance:  $\sigma^2 = pN_0$

# SNR



$$Contrast = \frac{\Delta I}{\bar{I}}$$
$$SNR = \frac{\Delta I}{\sigma_I} = \frac{C\bar{I}}{\sigma_I}$$

SNR Based on the number of photons (N):

then  $\Delta N$  describes the signal :

$$SNR = \frac{\Delta N}{\sigma_N} = \frac{\Delta N}{\sqrt{N}} = \frac{CN}{\sqrt{N}} = C\sqrt{N} \quad \text{where:} \quad C = \frac{\Delta N}{N}$$

# SNR based on Detected Photons per Pixel

The average number of photons  $N$  striking a detector depends on:

1- Source Output (Exposure), **Roentgen (R)** (Considering Geometric efficiency  $\Omega/4\pi$  (fractional solid angle subtended by the detector))

2- Photon Fluence/Roentgen  $\frac{\Phi}{R} = 2.5 \cdot 10^{10} \frac{\text{Photons} / \text{cm}^2}{R}$  for moderate energy

3- Pixel Area ( $\text{cm}^2$ )

4- Transmission probability  $p$

$$N = \Phi A R \exp\left[-\int \mu dz\right]$$



Let  $t = \exp[-\int \mu dz]$  and Add a recorder with quantum efficiency  $\eta$

$$SNR = C\sqrt{N} = C\sqrt{\eta\Phi ARt}$$

Example chest x-ray:

50 mRad = 50 mRoentgen

$\eta = 0.25$

Res = 1 mm

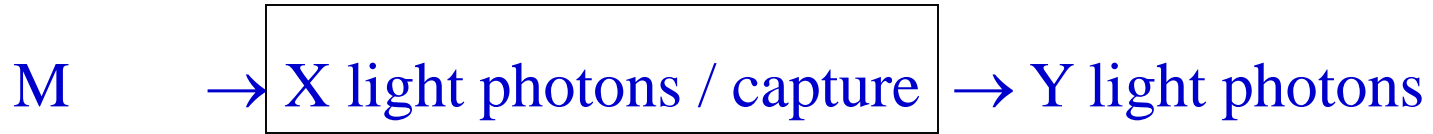
$t = 0.05$

What is the SNR as a function of C?

$$SNR = C\sqrt{N} = C\sqrt{\eta N}$$

# SNR based on Light Photons per Pixel on Film

Consider the detector



Captured Photons  
In Screen (Poisson)

What are the zeroth order statistics on Y?

$$Y = \sum_{m=1}^M X_m$$

Y depends on the number of x-ray photons M that hit the screen, a Poisson process.

Every photon that hits the screen creates a random number of light photons, also a Poisson process.

What is the mean of Y? ( This will give us the signal level in terms of light photons)

$$Y = \sum_{m=1}^M X_m$$

Mean

$$E[Y] = E\left[\sum_{m=1}^M X_m\right]$$

Expectation of a Sum is  
Sum of Expectations (Always).  
There will be M terms in sum.

$$E[Y] = E[X_1] + E[X_2] + \dots + E[X_m]$$

Each Random Variable X has same mean.

There will be M terms in the sum

$E[Y] = E[M] E[X]$  Sum of random variables

$E[M] = \eta N$  captured x-ray photons / element

$E[X] = g_1$  mean # light photons/single x-ray capture

so the mean number of light photons is  $E[Y] = \eta N g_1$ .

What is the variance of  $Y$ ? ( This will give us the std deviation)

$$Y = \sum_{m=1}^M X_m$$

We consider the variance in  $Y$  as a sum of two variances:

1. The first will be an uncertainty in  $M$ , the number of incident X-ray photons.
2. The second will be due to the uncertainty in the number of light photons generated per each X-ray photon,  $X_m$ .

What is the variance of Y due to M?

$$Y = \sum_{m=1}^M X_m$$

Considering M (x-ray photons) as the only random variable and X (Light/photons) as a constant,

then the summation would simply be:

$$Y = MX.$$

The variance of Y is:

$$\sigma_y^2 = X^2 \sigma_M^2$$

(Recall that multiplying a random variable by a constant increases its variance by the square of the constant. Note: The variance of M effects X)

But X is actually a Random variable, so we will write X as E[X]

Therefore, Uncertainty due to M is:  $\sigma_{y1}^2 = [E[X]]^2 \sigma_M^2$

What is the variance of Y due to X (Light/photons)?  $Y = \sum_{m=1}^M X_m$

Here, we consider each  $X$  in the sum as a random variable but  $M$  is considered fixed:

Then the variance of the sum of  $M$  random variables would simply be  $M \cdot \sigma_x^2$

Note: Considering that the variance of  $X$  has no effect on  $M$  (ie. each process that makes light photons by hitting a x-ray photon is independent of each other)

Therefore, Uncertainty due to  $X$  is:  $\sigma_{y^2}^2 = E[M] \sigma_x^2$

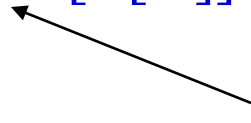
$$\sigma_M^2 = \mathbf{E} [M] = \eta N$$

Recall M is a Poisson Process

$$\sigma_X^2 = \mathbf{E} [X] = g_1$$

Generating light photons is also Poisson

$$\sigma_Y^2 = \sigma_{y1}^2 + \sigma_{y2}^2 = [\mathbf{E}[X]]^2 \sigma_M^2 + \mathbf{E}[M] \sigma_X^2 = \eta N g_1^2 + \eta N g_1$$



Uncertainty of Y due to M

Uncertainty of Y due to X

$$SNR = \frac{CE[Y]}{\sigma_y} = \frac{C\eta N g_1}{\sqrt{\eta N g_1 + \eta N g_1^2}} = \frac{C\eta N g_1}{\sqrt{\eta N g_1} \sqrt{1 + g_1}}$$

Dividing numerator and denominator by  $g_1$

$$= \frac{C\sqrt{\eta N}}{\sqrt{1 + \frac{1}{g_1}}}$$

What can we expect for the limit of  $g_1$ , the generation rate of light photons?

$$g_1 = \frac{h\nu_{x\text{-ray}}}{h\nu_{\text{light}}} = \frac{\lambda_{\text{light}}}{\lambda_{x\text{-ray}}} = \frac{5000 \text{ \AA}}{.25 \text{ \AA}} \approx 20,000$$

Actually, half of photons escape and energy efficiency rate of screen is only 5%. This gives us a  $g_1 = 500$

Since  $g_1 \gg 1$ ,  $SNR \approx C\sqrt{\eta N}$



# SNR based on Density grains per Pixel on Film

We still must generate pixel grains

$$W = \sum_{m=1}^Y Z_m \text{ where } W \text{ is the number of silver grains developed}$$

$$Y \rightarrow \boxed{Z} \rightarrow W \text{ grains / pixel}$$

Light  
Photons /  
pixel

$Z = \text{developed Silver grains / light photons}$

Let  $E[Z] = g_2$ , the number of light photons to develop one grain of film.

Then,  $\sigma_z^2 = g_2$  (since this is a Poisson process, i.e. the mean is the variance).

$$E[W] = E[Y] E[Z] = \eta N g_1 \cdot g_2$$

$$\text{Recall: } \sigma_Y^2 = \eta N g_1^2 + \eta N g_1$$

$$E[Z] = \sigma_z^2 = g_2 \quad \text{Number of light photons needed to develop a grain of film}$$

$$\sigma_w^2 = \underbrace{\sigma_Y^2 E^2[Z]}_{\text{uncertainty in light photons}} + \underbrace{E[Y] \sigma_z^2}_{\text{uncertainty in gain factor } z}$$

$$\sigma_w^2 = (\eta N g_1^2 + \eta N g_1) g_2^2 + g_1 \eta N g_2$$

$$\sigma_w = g_1 g_2 \sqrt{\eta N} \sqrt{1 + 1/g_1 + 1/g_1 g_2}$$

$$SNR = \frac{CE[W]}{\sigma_w} = \frac{C \sqrt{\eta N}}{\sqrt{1 + 1/g_1 + 1/g_1 g_2}}$$

Recall  $g_1 = 500$  (light photons per X-ray)

$g_2 = 1/200$  light photon to develop a grain of film

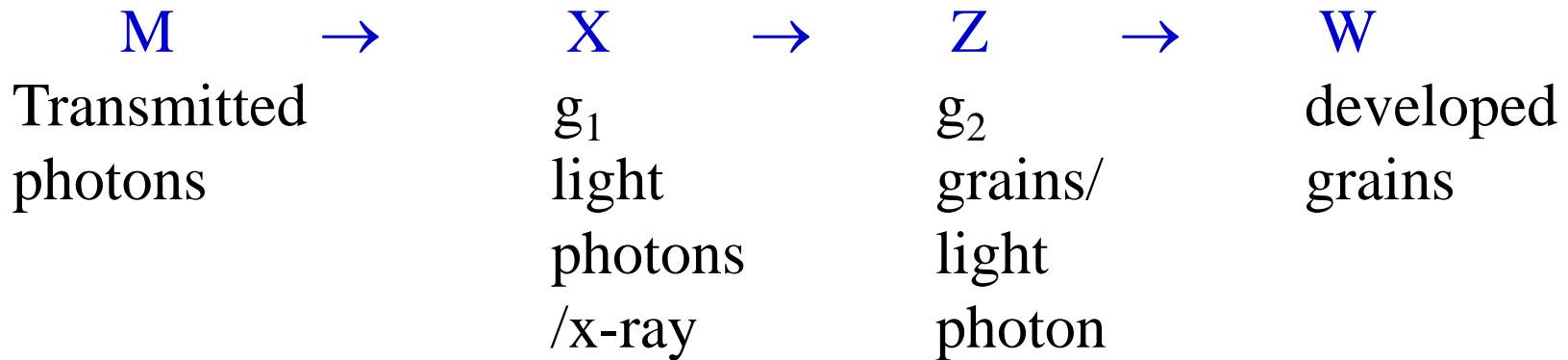
That is one grain of film requires 200 light photons.

$$1/g_1 \ll 1$$

$$SNR = \frac{C\sqrt{\eta N}}{\sqrt{1 + 1/500 + \frac{1}{500 \cdot 200}}}$$

$$SNR \approx 0.85C\sqrt{\eta N}$$

# Putting it all together...

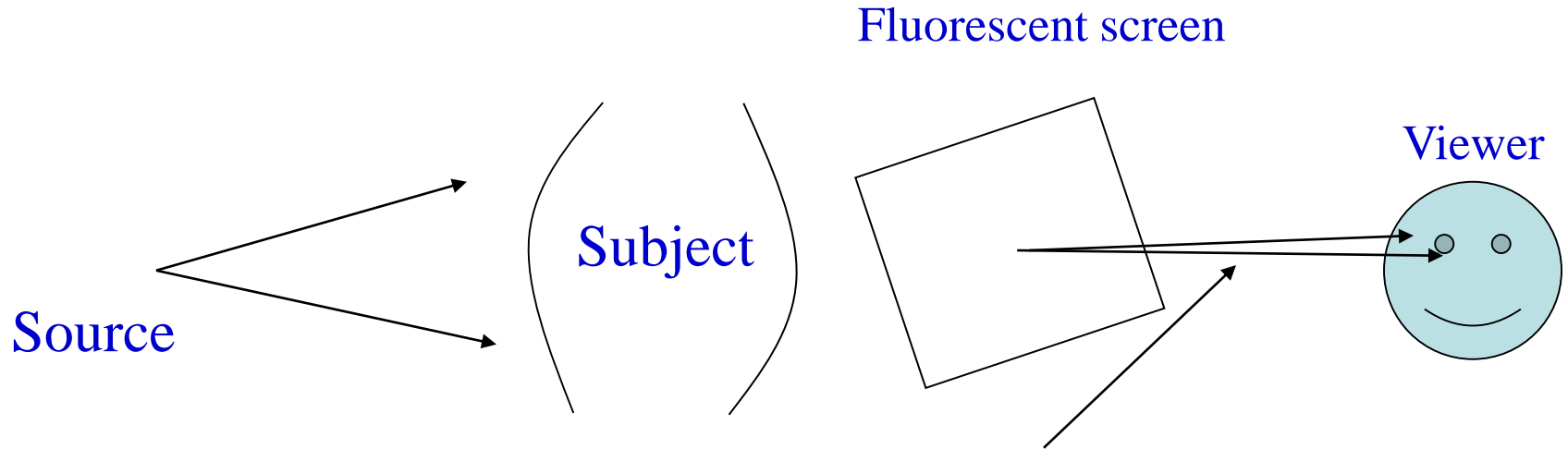


For  $N$  as the average number of transmitted, not captured, photons per unit area.

$$SNR = \frac{C\sqrt{\eta N}}{\sqrt{1 + 1/g_1 + 1/g_1 g_2}}$$

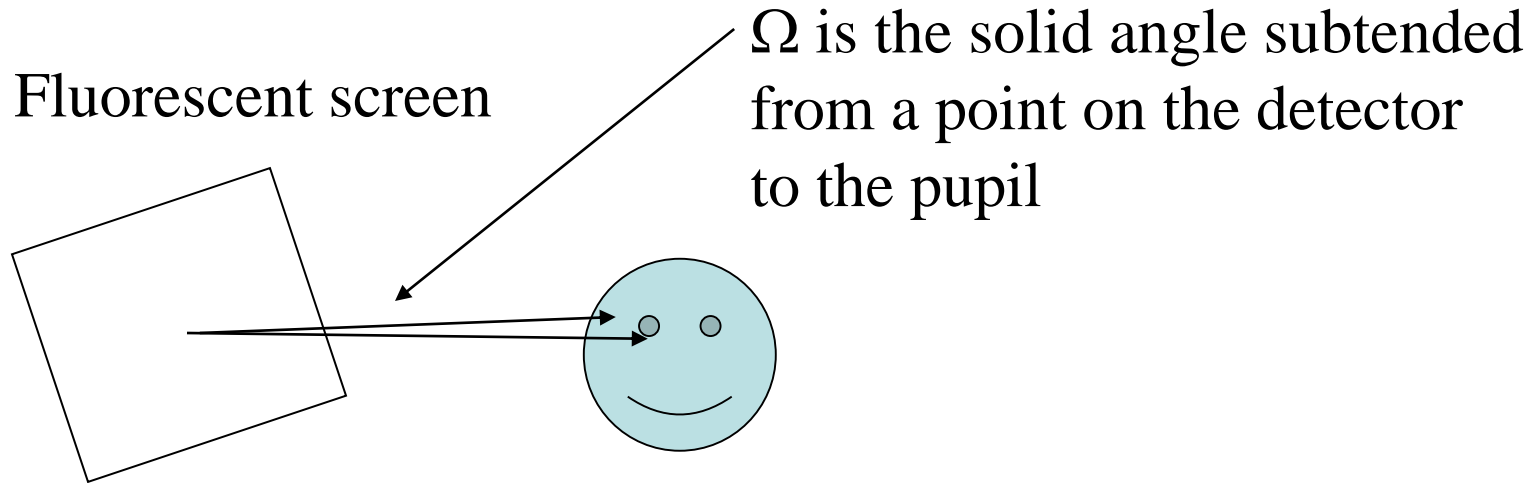
# Fluoroscopy

-Old Method



$\Omega$  is the solid angle subtended from a point on the detector to the pupil

If a fluorescent screen is used instead of film, the eye will only capture a portion of the light rays generated by the screen.  
How could the eye's efficiency be increased?



Let's calculate the eye's efficiency capturing light  $\eta_\varepsilon$

$$\eta_\varepsilon = \frac{\Omega}{4\pi} T_e = \frac{A}{4\pi r^2} T_e$$

$r$  = viewing distance (minimum 20 cm)

$T_e$   $\equiv$  retina efficiency ( approx. 0.1)

$A$  = pupil area  $\approx 0.5 \text{ cm}^2$  (8 mm pupil diameter)

Recall

$$SNR = \frac{C\sqrt{\eta N}}{\sqrt{1 + 1/g_1 + 1/g_1 g_2}}$$

In fluoroscopy:

$g_1 = 10^3$  light photons / x-ray

$g_2 = \eta_\epsilon$

$\eta_\epsilon \approx 10^{-5}$  (at best)      Typically  $\eta_\epsilon \approx 10^{-7}$

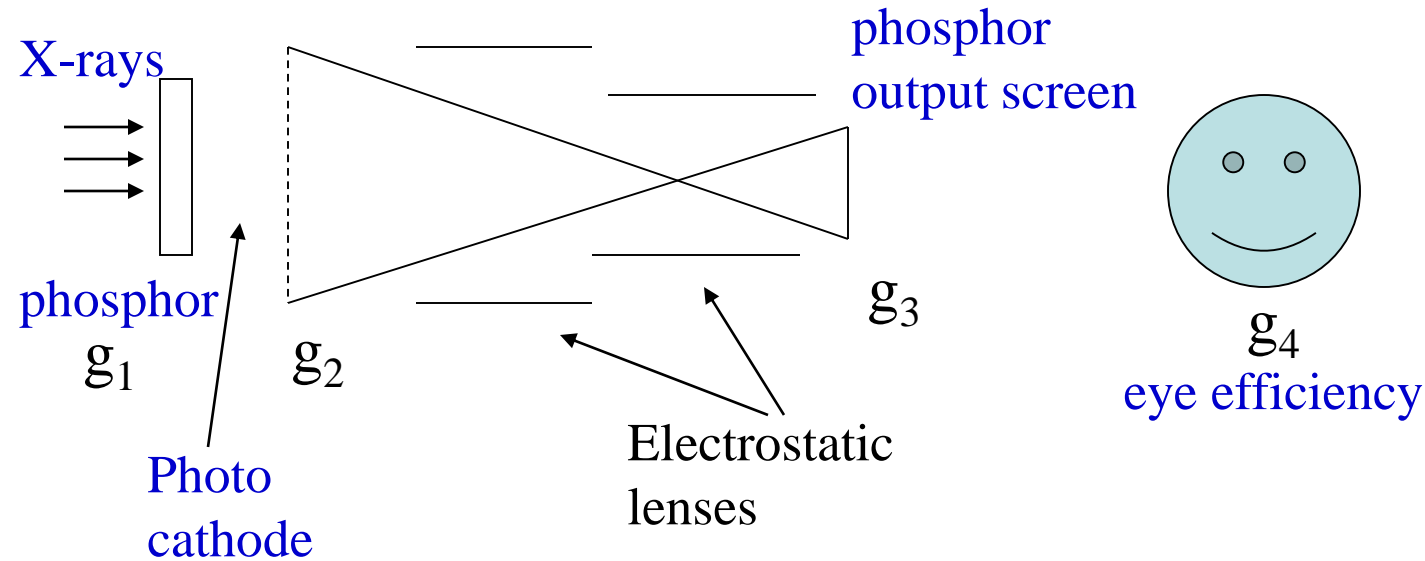
$g_1 g_2 = 10^3 10^{-5} = 10^{-2}$  at best

Therefore loss in SNR is about 10

We have to up the dose by a factor of 100! (or, more likely, to compromise resolution rather than dose)

At each stage, we want to keep the gain product  $\gg 1$  or quantum effects will harm SNR.

# Image Intensifier



$g_1$  = Conversion of x-ray photon to Light photons in Phosphor

$g_2$  = Conversion of Light photons into electrons

$g_3$  = Conversion of accelerated electron into light photons

$$SNR = \frac{C\sqrt{\eta N}}{\sqrt{1 + \frac{1}{g_1} + \frac{1}{g_1 g_2} + \frac{1}{g_1 g_2 g_3} + \frac{1}{g_1 g_2 g_3 g_4}}}$$



$g_1 = 10^3$  light photons / captured x-ray

$g_2 = \text{Electrons} / \text{light photons} = 0.1$

$g_1 g_2 = 100$

$g_3 = \text{emitted light photons} / \text{electron} = 10^3$

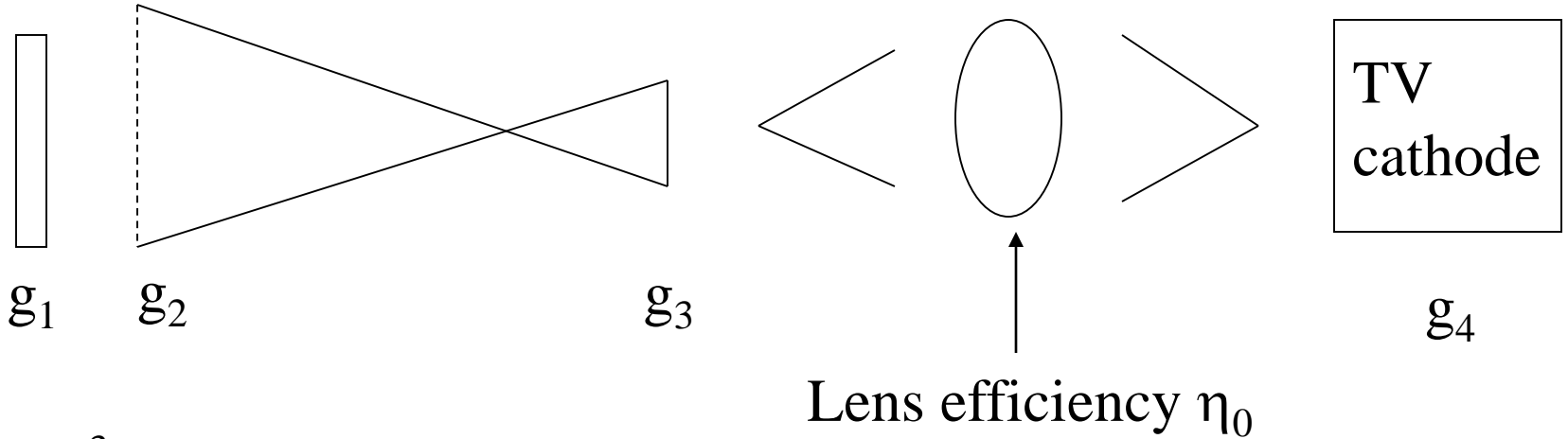
$g_4 = \eta_\varepsilon \text{ eye efficiency} = 10^{-5} \text{ optimum}$

$g_1 g_2 g_3 g_4 = 10^3 10^{-1} 10^3 10^{-5} = 1$

$$SNR = \frac{C \sqrt{\eta N}}{\sqrt{1 + \frac{1}{g_1} + \frac{1}{g_1 g_2} + \frac{1}{g_1 g_2 g_3} + \frac{1}{g_1 g_2 g_3 g_4}}}$$

$$SNR_{\text{loss}} = \frac{1}{\sqrt{1+1}} = \sqrt{2} / 2$$

# Add a TV



$$g_1 = 10^3$$

$$g_2 = 10^{-1}$$

$$g_3 = 10^3 \eta_0$$

$\eta_0 \approx 0.04$  (Lens efficiency. Much better than eye)

$g_4 = 0.1$  electrons / light photon

$$g_1 g_2 g_3 g_4 = 4 \times 10^2$$

$$g_1 g_2 g_3 g_4 \gg 1$$

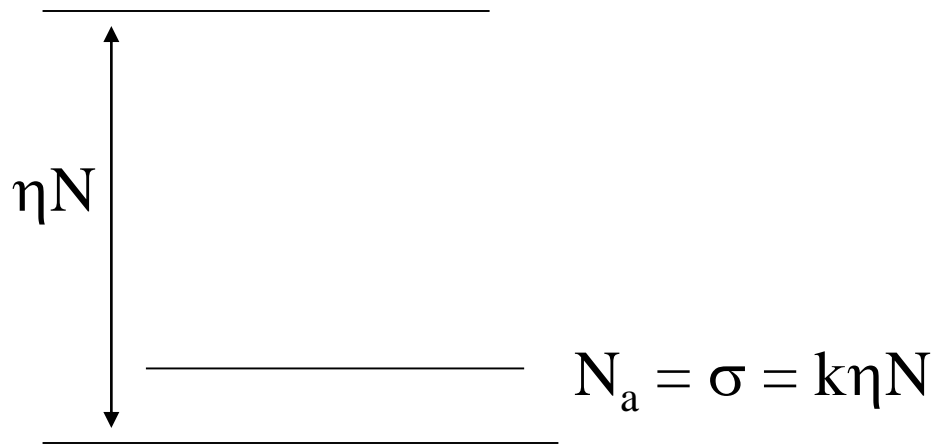
and all the intermediate gain products  $\gg 1$

$$SNR = C \sqrt{\eta N}$$

# Additive TV Noise

But TV has an additive electrical noise component.  
Let's say the noise power (variance) is  $N_a^2$ .

$$SNR = \frac{C\eta N}{\sqrt{\eta N + N_a^2}}$$



- In X-ray, the number of photons is modeled as our source of signal.
- We can consider  $N_a$  (which is actually a voltage), as its equivalent number of photons.
- Electrical noise then occupies some fraction of the signal's dynamic range. Let's use  $k$  to represent the portion of the dynamic range that is occupied by additive noise.

$$SNR = \frac{C\eta N}{\sqrt{\eta N + k^2\eta^2 N^2}} = \frac{C\eta N}{\eta N \sqrt{\frac{1}{\eta N} + k^2}} = \frac{C}{k} \sqrt{\frac{1}{1 + 1/k^2\eta N}}$$

# Typical TV

$$SNR = \frac{C}{k} \sqrt{\frac{1}{1 + 1/k^2 \eta N}}$$

$$k = 10^{-2} \text{ to } 10^{-3}$$

$$\eta N = 10^5 \text{ photons / pixel}$$

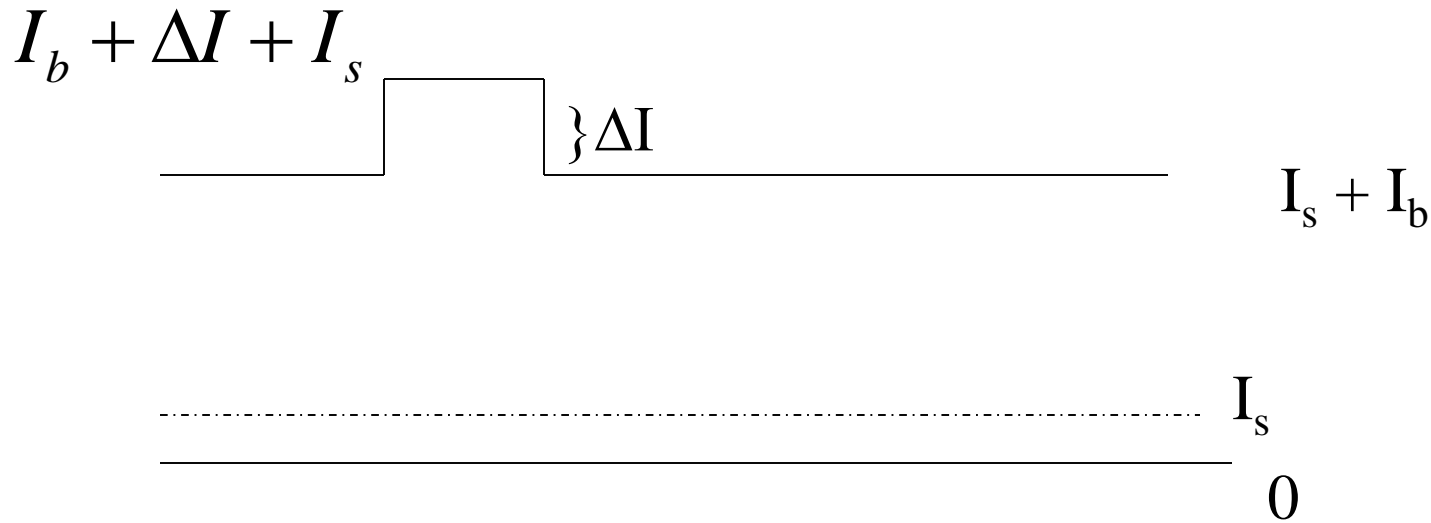
$$k = 10^{-2} \quad k^2 \eta N = 10$$

$$k = 10^{-3} \quad k^2 \eta N = 10^{-1} \quad \text{Much Better!}$$

$$\text{If } k^2 \eta N \ll 1 \quad SNR = C \sqrt{\eta N}$$

$$\text{If } k^2 \eta N \gg 1 \quad SNR \approx C/k \quad \text{poor, not making use of radiation}$$

# Scatter Radiation



Scatter increases the background intensity.

Scatter increases the level of the lesion.

Let the ratio of scattered photons to desired photons be

$$\psi = \frac{I_s}{I_b}$$

$$C_s = \frac{(I_b + \Delta I + I_s) - (I_s + I_b)}{I_s + I_b}$$

$$C_s = \frac{\Delta I}{I_s + I_b} = \frac{\Delta I}{I_b \left(1 + \frac{I_s}{I_b}\right)} = \frac{C}{\left(1 + \frac{I_s}{I_b}\right)}$$

Let  $\psi = \frac{I_s}{I_b}$  then  $C_s = \frac{C}{1 + \psi}$

# SNR Effects of Scatter

The variance of the background depends on the variance of transmitted and scattered photons.

Both are Poisson and independent so we can sum the variances.

$\sigma_N^2 = \eta N + \eta N_s$  where  $N_s$  is mean number of scattered photons

$$SNR = \frac{C \eta N}{\sqrt{\eta N + \eta N_s}} = C \frac{\sqrt{\eta N}}{\sqrt{1 + \frac{N_s}{N}}} = C \frac{\sqrt{\eta N}}{\sqrt{1 + \Psi}}$$

Here  $C$  is the scatter free contrast.



# Filtering of Noisy Images

- Imaging system is combination of Linear filters with in turn effects on Noisy signals
- Noise can be Temporal or Spatial in an image
- This can also be classified as Stationary or nonstationary
- If the Random fluctuating input to a system with impulse response of  $p(t)$  is  $w_{in}(t)$ , what can be the mean  $\langle w_{out} \rangle$  and variance  $\sigma_{out}$  of the output (which is noise variation):